Hara et al. Dynamic Cardiac Phantom with a Double Pump

Development of Two-layered Dynamic Cardiac Phantom Made of Double Pump

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ABSTRACT

The conventional dynamic cardiac phantom used in the field of nuclear medicine has a structure where the size of the external side of the heart (the outer membrane substituting the myocardial layer) is fixed and only the inner side (the inner membrane substituting the ventricle part) moves anteroposteriorly. Therefore, its usefulness in technical evaluation is limited. Hence, we report that we developed a new dynamic cardiac phantom where the outer and inner membranes freely move.

Methods: By using the single-photon emission computed tomography and computed tomography (SPECT/CT) system (Precedence 16, Philips), we performed validation by filling the myocardial layer of the dynamic cardiac phantom with solution and the ventricle part with contrast medium. We evaluated myocardial wall motions of three segments (basal, mid, and apical) by setting the stroke ratios at 20:20 and 10:10 (ventricle-to-myocardial layer ratio).

Results: The myocardial wall motions (mean \pm SD) at the stroke ratio of 20:20 were 7.50 \pm 0.44, 11.15 \pm 0.56, and 9.90 \pm 0.24 mm in the basal, mid, and apical segments, respectively. The wall motions (mean \pm SD) at the stroke ratio of 10:10 were 3.82 \pm 0.43, 5.63 \pm 0.39, and 4.53 \pm 0.10 mm, respectively.

Conclusions: In our dynamic cardiac phantom, different movements could be induced in the myocardial wall by freely changing the stroke ratio. These results suggest that the use of this phantom can realize technical evaluation that presumes various clinical conditions.

Key words: Dynamic cardiac phantom, Myocardial wall movement, Gated myocardial SPECT, SPECT/CT

INTRODUCTION

Nuclear medicine examination using gated myocardial single-photon emission computed tomography (gated myocardial SPECT) can provide image information of high clinical usefulness as a functional diagnostic method [1-5] and much evidence for the diagnosis of ischemic heart disease [6-8], severity assessment [9,10], determination of treatment efficacy [11,12], prognosis prediction, and risk stratification [13-15]. In order to secure and establish evidence, technical evaluation is needed as a basic study. However, the conventional dynamic cardiac phantom used for technical evaluation of gated myocardial SPECT [16] has a structure where the size of the external side of the heart (the outer membrane substituting the myocardial layer) is fixed and only the inner side (the inner membrane substituting the ventricle) moves anteroposteriorly (FIGURE 1A). Therefore. detailed technical evaluation corresponding to actual clinical conditions cannot be performed. In order to perform technical evaluation toward clinical application, we report that we developed a new dynamic cardiac phantom where the outer and inner membranes move freely (FIGURE 1B,2A). The myocardial layer is comprised of outer and inner membranes made of special rubber, and heart movement is reproduced by using two cylinder pumps (FIGURE 2B). The outlet (discharge outlet: 15) for solutions supplied to the area of the ventricle and myocardial layer (e.g., radioactive and contrast agents) has a special structure (FIGURE 2C). The contents of the ventricle and myocardial layer can be changed by setting the stroke ratio of the cylinder pumps freely (FIGURE 2D).

MATERIALS AND METHODS

Setting of the Phantom

The movable parts of the myocardial layer and ventricle in the new dynamic cardiac phantom were filled with a mixed solution of radioactive agent (755.00 mL of distilled water and 0.74 MBq/mL ^{99m}TC solution) and contrast agent (982.00 mL of distilled water and 370 mg/mL of iodine concentration), respectively. Table 1 shows the actual measurement values calculated from the structure of the new dynamic cardiac phantom (end-diastolic volume [EDV], end-systolic volume [ESV], and left ventricular

ejection fraction [LVEF]).

At the time of SPECT data acquisition, the heart rate was fixed at 60 bpm and 11 patterns of stroke ratio (ventricle-to-myocardial layer ratio) were set (20:20, 20:10, 20:5, 15:15, 15:10, 15:5, 10:10, 10:5, 10:20, 10:15, and 5:10).

Gated SPECT data acquisition and image reconstruction

A SPECT/CT system (Precedence 16, Philips) was used. The conditions for gated SPECT data acquisition were data acquisition time at 30 sec/step (360°, 64 steps), R-R interval at 16, use of a vertex general-purpose collimator, matrix sizes of 128 \times 128 (pixel size, 3.19 mm) and 64 \times 64 (6.39 mm) (concurrent imaging: different acquisition data can be stored at one imaging).

Gated myocardial perfusion image reconstruction was performed by using filtered back projection as the reconstruction method (cutoff of 0.19 cycles/cm and order 9 for a matrix size of 128×128) and a Butterworth filter for the preprocessing filter (cutoff of 0.37 cycles/cm and order 9 for a matrix size of 64×64). A ramp filter was used as the reconstruction filter, without attenuation correction and scatter correction.

Analysis

Results of the cardiac function analysis of the SPECT data (EDV, ESV, LVEF, myocardial wall motion, and changes in wall thickness) were processed by using EBW-NM4.5 (Philips). The Statistical Package for Social Sciences software (IBM) was used for the statistical analysis.

RESULTS

Table 1 shows the actual measurement values obtained by using our new dynamic cardiac phantom and the EDV, ESV, and LVEF analyzed from the SPECT images. FIGURE 3 (A, B, and C) shows the results of the statistical analysis. In the comparison between the actual measurement values and the SPECT analysis values, high correlations were observed in matrix size 128 (EDV, r = 0.92; ESV, r = 0.93; LVEF,

r = 0.95) and matrix size 64 (EDV, r = 0.90; ESV, r = 0.88; LVEF, r = 0.95).

FIGURE 4 (A and B) shows the results of the myocardial wall motion at each stroke ratio. The wall motions at each stroke ratio were within the ranges of 2.13 to 7.50 mm, 3.32 to 11.10, and 3.00 to 9.90 mm in the basal, mid, and apical segments, respectively, for matrix size 128, and 2.10 to 7.87 mm, 3.23 to 11.27 mm, and 3.05 to 10.25 mm, respectively, for matrix size 64 (FIGURE 4).

FIGURE 5 shows the results of the changes in wall thickness at each stroke ratio.

The maximum and minimum changes in wall thickness at each stroke ratio (mean \pm SD) for matrix size 128 were 16.55 \pm 1.56 and 5.47 \pm 0.64 mm, 11.35 \pm 3.29 and 2.45 \pm 0.85 mm, and 9.73 \pm 2.91 and 2.75 \pm 1.48 mm in the basal, mid, and apical segments, respectively, and those for matrix size 64 were 17.90 \pm 1.66 and 5.87 \pm 0.65 mm, 12.83 \pm 3.49 and 2.67 \pm 1.03 mm, and 10.90 \pm 3.14 and 2.88 \pm 1.45 mm, respectively (FIGURE 5A,B).

DISCUSSION

The usefulness of gated myocardial SPECT in the quantitative evaluation of transient left ventricular dysfunction and myocardial blood flow impairment has been reported, and it has improved the accuracy of evaluations of severity [9, 10], risk, and prognosis [13-15]. In addition, gated myocardial SPECT has been reported to be useful for the evaluation of EDV, ESV, LVEF, stroke volume/cardiac index, myocardial wall motion, and changes in myocardial wall thickness, which are critical in risk and prognosis assessment in coronary artery diseases [1,2]

Published reports have stated that application of the exercise or drug loading method by using gated myocardial SPECT can quantitatively evaluate markers of poor prognosis, transient reduction in LVEF after loading and myocardial wall motion abnormality [3,4]. These reports suggest the need of further improvement of the technical accuracy of nuclear cardiology examinations.

Recent advances have led to the development of nuclear cardiology devices mounted with a semiconductor detector, and technical evaluation was performed on these devices [17-19]. However, the phantoms used in the previous studies were

static cardiac phantoms [17] and cardiac SPECT phantoms [19]. With these phantoms, detailed technical evaluation with gated myocardial SPECT cannot be performed. We developed a new dynamic cardiac phantom because the evaluation of myocardial wall motion is considered necessary, in addition to the evaluation of EDV, ESV, and LVEF, to perform technical evaluation with high clinical applicability in the future.

Detailed cardiac function analysis cannot be performed with static cardiac phantoms used for technical evaluation in nuclear cardiology examinations [20-22] or the conventional dynamic cardiac phantom developed by Kubo N et al. [16], where cardiac function analytical values (EDV, ESV, and LVEF) are fixed values calculated from the forms of the phantoms. However, the actual measurement values at the different stroke ratios of our new dynamic cardiac phantom showed high correlation with SPECT analysis values, suggesting that detailed validation of cardiac function analysis can be performed by setting stroke ratios appropriate for clinical application (TABLE 1, FIGURE 5).

The dynamic myocardial phantoms reported by Jacco JN et al. [23] and Luca et al. [24] have two discharge outlets for solution supplied to the myocardial layer, and the same pump is used to supply solution to the ventricle part and myocardial layer. Although EDV, ESV, and LVEF were evaluated, no detailed evaluation was performed such as that for myocardial wall motion. In our new dynamic cardiac phantom, the solution supply system to the myocardial layer has a special structure (FIGURE 2C, discharge outlet 15). It has independent supply pumps to the ventricle and myocardial layer (FIGURE 2B), and stroke ratios can be set freely (FIGURE 2D). In addition to the evaluation of EDV, ESV, and LVEF at different stroke ratios (FIGURE 3), various myocardial wall motions can be set through the combination of stroke ratios of the cylinder pumps of the ventricle and myocardial layer (FIGURE 4). Among the stroke ratios validated, we could confirm free changes in myocardial wall thickness based on the differences between 20:10 and 10:20 (2.54, 6.97, and 4.63 mm in the basal, mid, and apical segments, respectively), between 15:10 and 10:15 (1.15, 3.26, and 2.33) mm, respectively), and between 10:5 and 5:10 (0.28, 2.78, and 1.45 mm, respectively; (FIGURE 5).

CONCLUSION

This study demonstrates that our new dynamic cardiac phantom can be used for technical evaluation that presumes various clinical conditions. Technical validation for SPECT image processing and attenuation correction using this phantom is needed in the future.

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FIGURE 1. A: Schematic diagram of conventional dynamic cardiac phantom for nuclear medicine. B: Schematic diagram of new dynamic cardiac phantom for nuclear medicine.



FIGURE 2. A: Our new dynamic cardiac phantom. B: Appearance of the two cylinder pumps. D: Appearance of the outlet (front). E: The scale of the stroke.



FIGURE 3. Results of the statistical analysis of the actual measurement values and SPECT analysis values. A: EDV; B: ESV; and C: LVEF.



FIGURE 4. Results of the stroke ratios and wall motion. A: Matrix size, 128×128 . B: Matrix size, 64×64 .



FIGURE 5. Results of the stroke ratios and changes in myocardial wall thickness. A: Matrix size, 128×128 . B: Matrix size, 64×64 .

	EDV (mL)			ESV (mL)			LVEF (%)		
	Actual	SPECT		Actual	SPECT		Actual	SPECT	
Stroke rate	measurement value	128x128	64x64	measurement value	128x128	64x64	measurement value	128x128	64x64
20:20	495.76	506.00	489.00	294.80	276.00	257.00	40.60	45.50	47.40
20:10	495.76	473.00	465.00	294.80	271.00	262.00	40.60	42.70	43.70
20:05	495.76	468.00	450.00	294.80	286.00	269.00	40.60	38.90	40.20
15:15	470.64	459.00	430.00	319.90	289.00	264.00	32.03	37.00	38.60
15:10	470.64	451.00	438.00	319.90	292.00	285.00	32.03	35.30	34.90
15:05	470.64	445.00	414.00	319.90	303.00	270.00	32.03	31.90	34.80
10:10	445.52	430.00	416.00	345.00	319.00	304.00	22.56	25.80	26.90
10:05	445.52	425.00	410.00	345.00	333.00	317.00	22.56	21.60	22.70
10:20	445.52	440.00	416.00	345.00	311.00	282.00	22.56	29.30	32.20
10:15	445.52	432.00	421.00	345.00	306.00	297.00	22.56	29.20	29.50
5:10	420.40	404.00	385.00	370.16	336.00	321.00	11.95	16.80	16.60

TABLE 1. Actual measurement values and SPECT analysis values (EDV, ESV, and LVEF) at different stroke ratios.